

# Evaluating Lateral Pinch Force Across the Lifespan through Scaled Musculoskeletal Models of the Hand

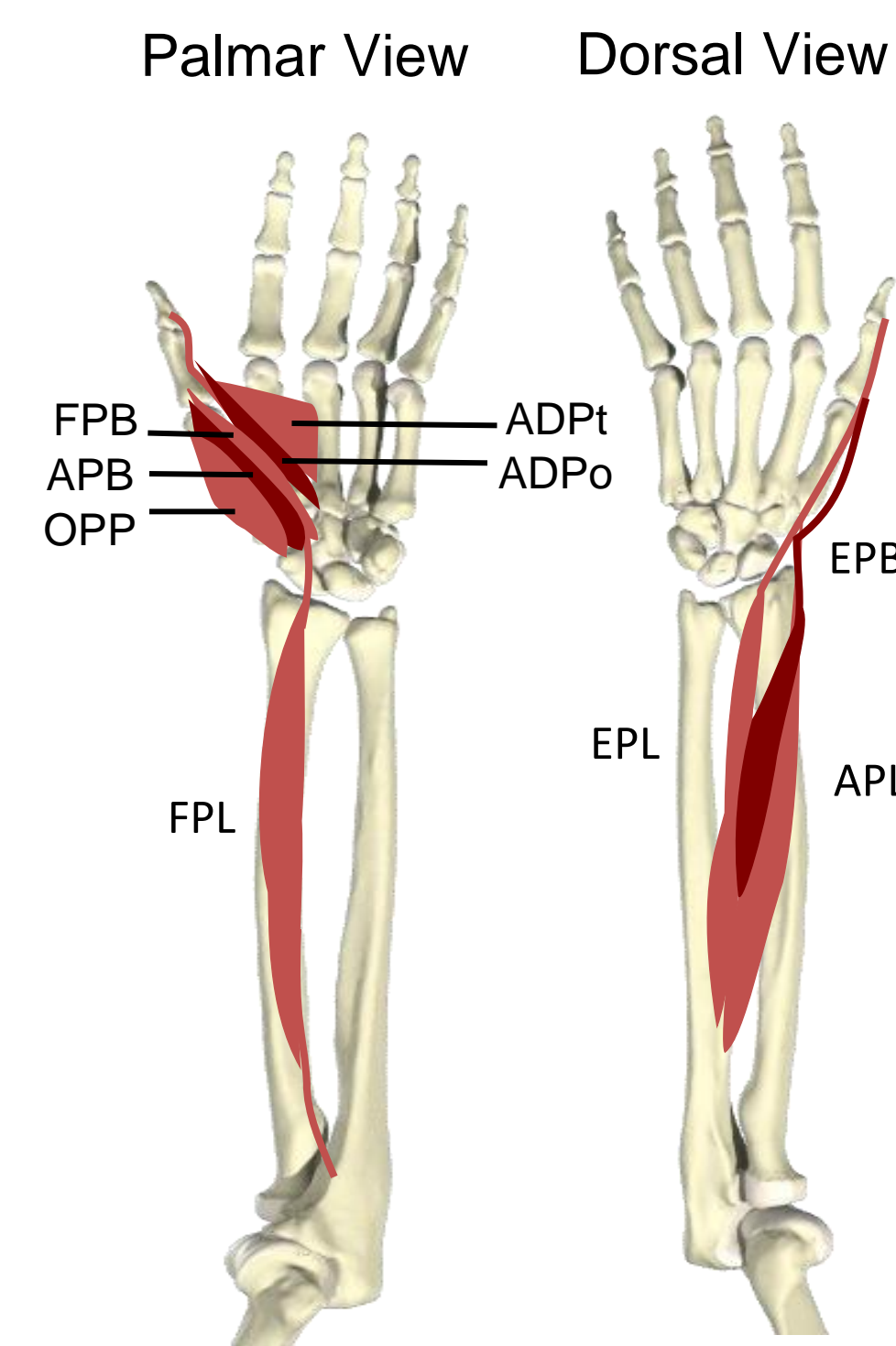


## INTRODUCTION

- Musculoskeletal models of the hand have given us a deeper understanding of hand function, motor control, and joint loading.<sup>1,2</sup>
- Pinch strength is an objective index of upper limb function and is used clinically as an indicator for treatment and rehabilitation.<sup>3</sup>
- For a model to accurately represent the diversity of the population, parameters such as age, biological sex, anthropometric measurements, and neuromuscular disorders need to be incorporated.

### Types of Musculoskeletal Models

- |   |                                     |  |
|---|-------------------------------------|--|
| <p><i>Subject-Specific Models</i> <sup>4,5</sup></p> <ul style="list-style-type: none"> <li>Improved accuracy</li> <li>Time and cost inefficient</li> </ul> | <p><b>Scaled generic models</b></p> | <p><i>Generic Models</i> <sup>4,5</sup></p> <ul style="list-style-type: none"> <li>Represent average adult males</li> <li>Low accuracy due to individual variation in musculoskeletal geometry and tissue</li> </ul> |
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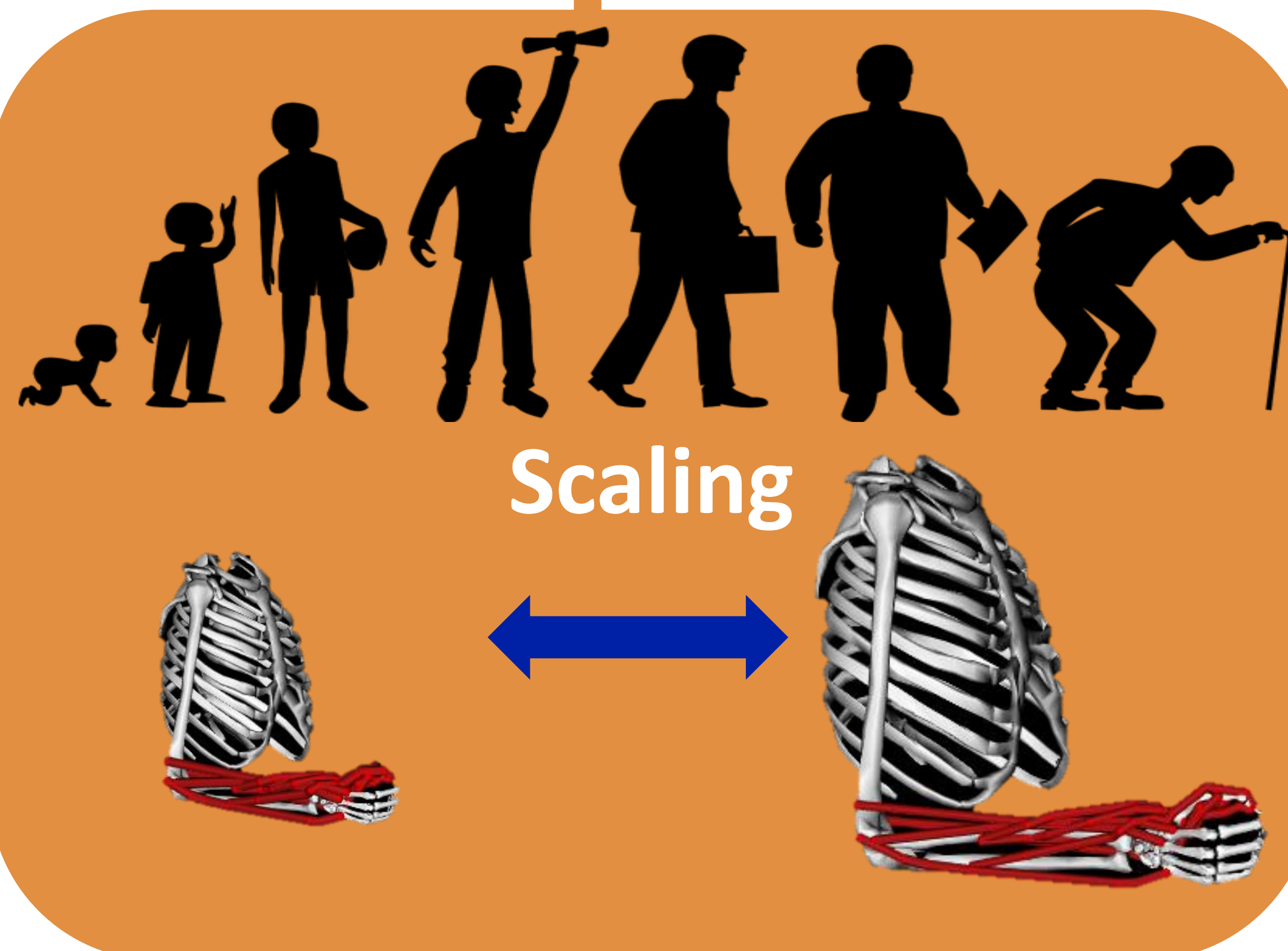
### Types of Scaling

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|--|-----------------------|---|
| <p><i>Linear Scaling</i> <sup>6,7</sup></p> <ul style="list-style-type: none"> <li>Anthropometric measurements:                     <ul style="list-style-type: none"> <li>Height, weight, BMI</li> </ul> </li> <li><b>Assumption:</b> Force-size relationship is the same across individuals</li> </ul> | <p><b>Scaling</b></p> | <p><i>Nonlinear Scaling</i> <sup>7,8</sup></p> <ul style="list-style-type: none"> <li>Digitization of medical images:                     <ul style="list-style-type: none"> <li>Computed tomography (CT)</li> <li>Magnetic resonance imaging (MRI)</li> </ul> </li> <li>Bone geometries and muscle volume meshes from cadaveric specimens</li> </ul> |
|--|-----------------------|---|

**Objective:** Evaluate how well scaled, generic, hand models performing pinch simulations represent differences in age.

## METHODS

- Musculoskeletal Models** <sup>9</sup>:
  - 9 extrinsic and 5 intrinsic muscles of the wrist and thumb
  - 6 degrees-of-freedom (2 at wrist and 4 across thumb)
  - Initial thumb position: 15° CMC extension, 20° CMC abduction, 20° MCP flexion, and 40° IP flexion
- Scaling of Models:**
  - Scaled to represent the full range of heights (1<sup>st</sup>, 15<sup>th</sup>\*, 50<sup>th</sup>, 80<sup>th</sup>, and 97<sup>th</sup> percentile) reported for four ages (7, 12, 16 and 30 years) <sup>4</sup>.
- Simulations:**
  - Lateral pinch force was measured for five sets of lateral pinch simulations using OpenSim (v. 3.3)
  - One-way ANOVA and Bonferroni procedure were used to compare simulation means for each color group (see below)

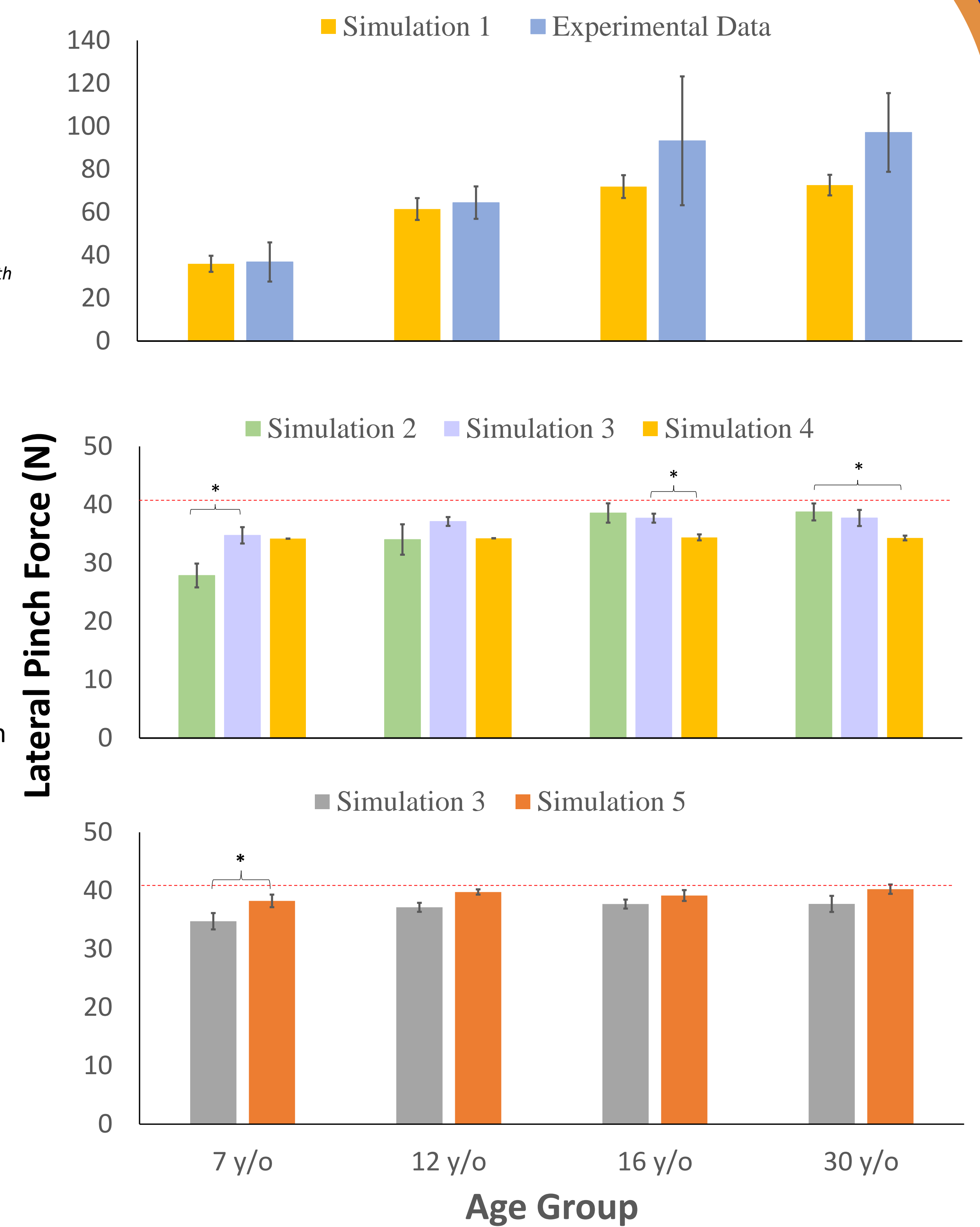


Comparison Groups	Maximum Pinch Strength		Muscle Control Strategy			Linearly Scaling
	Simulation 1	Experimental Data	Simulation 2	Simulation 3 <sup>a</sup>	Simulation 4	Simulation 5
<b>Input Config.</b>	50 <sup>th</sup> percentile male control strategy & maximally activating the FPL	Articles that have measured muscle control strategy during lateral pinch task	50 <sup>th</sup> percentile male control strategy	Unique muscle control strategy for each model	muscle activations controlled to match data collected through EMG	Muscle control strategy after doubling the max. iso. force
<b>Target Force</b>	Unconstrained	Unconstrained	40 N			40 N
<b>Descriptive Name</b>	FPL Exclusive	Experimental Data	Customary Control Strategy	Age-matched Control Strategy	Literature-based Control Strategy	Double Isometric Force
<b>Desired Output</b>	Max force	N/A	Effect of muscle control strategies on force achieved			Relationship between scaling and force output

<sup>a</sup> Simulation 3 was compared with the muscle control strategy and linearly scaled group

## RESULTS

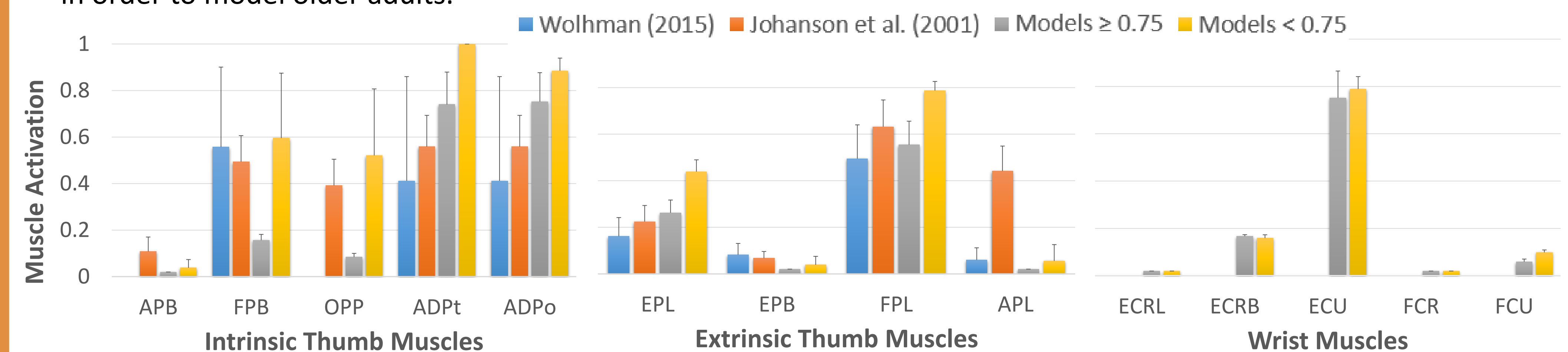
- Anthropometric scaling captured age-dependent differences in pinch strength
  - Simulations that *maximally activated the FPL* (Simulation 1) are not significantly different from the experimental data.
- Muscle activation strategies required to complete a task may shift as we age
  - 7 y/o model increased in pinch force from 50<sup>th</sup> percentile male control strategy simulations (Simulation 2) to the age-matched control strategy simulations (Simulation 3).
- Simulations can follow a similar muscle activation strategy as literature-based data
  - The *literature-based control strategy* simulations (Simulation 4) were able to reach completion.
- Simulations did not employ the optimal muscle fiber length to complete a pinch task
  - Doubling the max. isometric force (Simulation 5) did not double the lateral pinch force



## DISCUSSION

Anthropometrically scaled generic hand models have the potential to elucidate changes in strength across the lifespan.

- Together, the simulations enhance our knowledge of when anthropometric scaling can accurately represent differences in age.
  - The majority of scaled models were able to replicate experimental data and ran to completion.
  - However, the smaller scaled models (< 0.75, corresponding to below 132 cm height) implemented an unrealistic muscle control strategy to complete the task (see ECU activation in figure below) or failed to run to completion.
- Differences between simulations and experimental data could be attributed to the fact that model scaling assumes a linear correlation between model parameters and anthropometric data.
- Future research could explore how to incorporate age-related changes in muscle strength and/or activation patterns in order to model older adults.



More information can be found at: Ordonez Diaz, T., et al. 2021. *J Biomech*, 123, 110498. doi:10.1016/j.jbiomech.2021.110498.

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**REFERENCES:** [1] Mirakhorlo et al. 2018. *Comput Methods Biomech Biomed Eng*, 26:1-10. [2] Goislard et al. 2018. *Ann Biomed Eng*, 46:71-85. [3] Shin H., et al. 2012. *Ann Rehabil Med*, 36(3):394-399. [4] Song, K., et al. 2019. *Comput Methods Biomech Biomed Eng*, 22(3), 259-270. [5] Valero-Cuevas, F., et al. 2015. *J Biomech*, 48(11), 2887-2896. [6] Lund, M. E., et al. 2015. *International Biomechanics*, 2(1), 1-11. [7] Modenese, L., et al. 2016. *J Biomech*, 49(2), 141-148. [8] Nolte, D., et al. 2016. *J Biomech*, 49(14), 3576-3581. [9] Nichols, J., et al. 2017. *J Biomech*, 58:97-104.