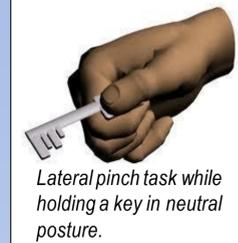
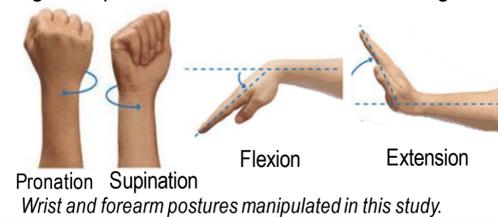


## Introduction



Lateral pinch task while holding a key in neutral posture.

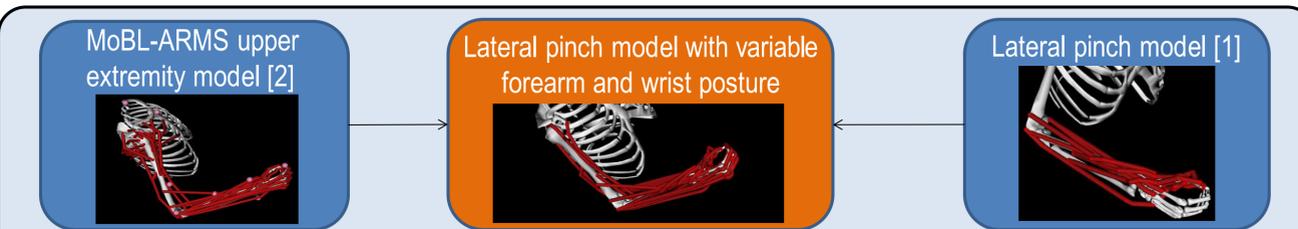
- The wrist and hand possess great versatility in grasping and manipulating objects, allowing humans to perform a variety of activities. However, forces generated by the hand during upper-limb tasks at various postures are not well understood [1].
- Simulations provide a unique tool to study how limb posture influences force generation, but simulations of force generation are typically run at a single, neutral posture.
- Understanding what postures result in excessive strength requirements can inform tool design and potentially prevent injury.



Pronation Supination Flexion Extension  
Wrist and forearm postures manipulated in this study.

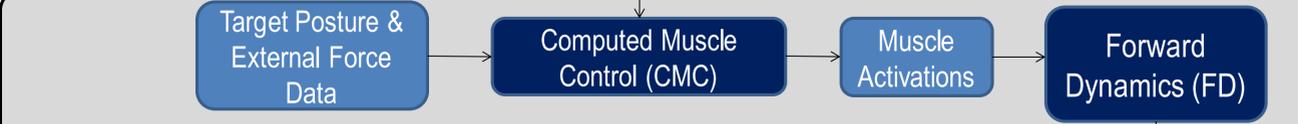
**OBJECTIVE:** To evaluate how **wrist and forearm posture** affect **thumb-tip force during lateral pinch** and compare simulated results with experimental literature in order to inform a model capable of predicting postures that require excessive strength inputs.

## Methods



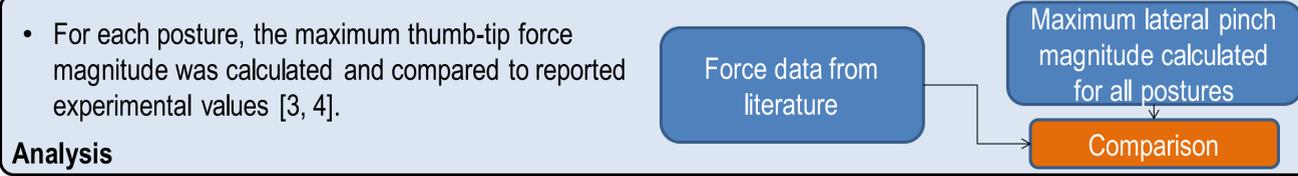
- A musculoskeletal model of the forearm, wrist, and thumb was created in OpenSim [v 3.3].
- This model importantly included 180° pronation/supination at the forearm and 140° flexion/extension at the wrist.

### Model Creation



- Simulations combined 5 forearm postures (-90° supination to 90° pronation in increments of 45°) and 5 wrist postures (-60° extension to 60° flexion in increments of 30°).

### Simulations

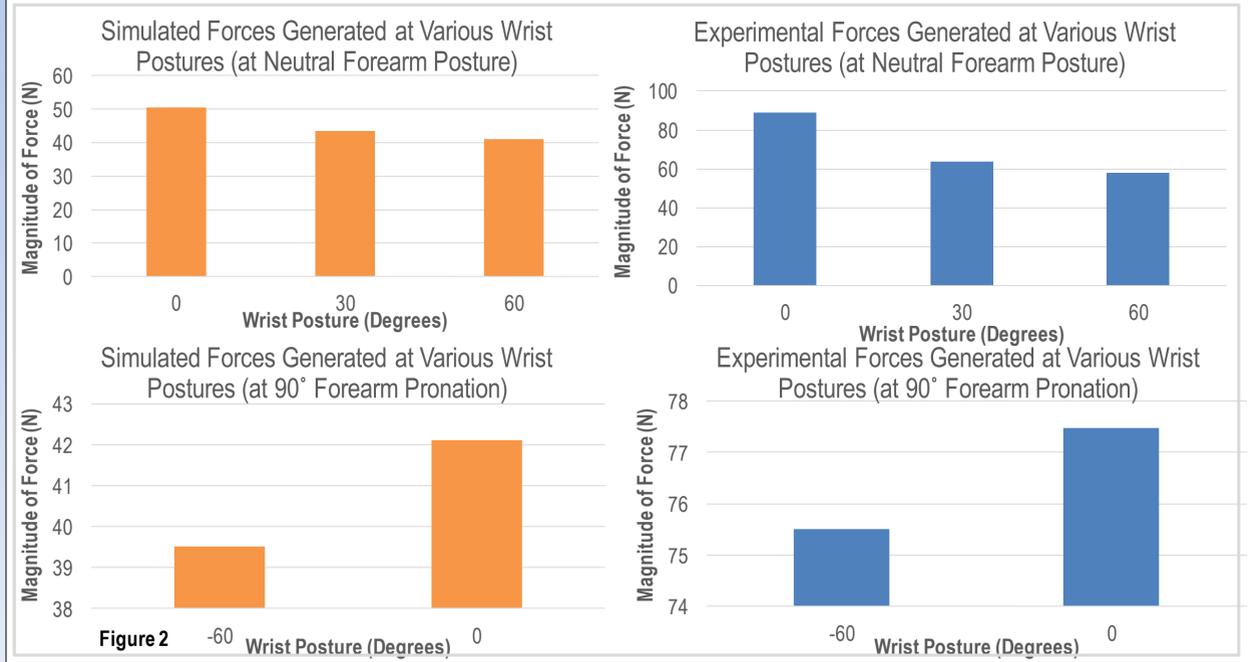
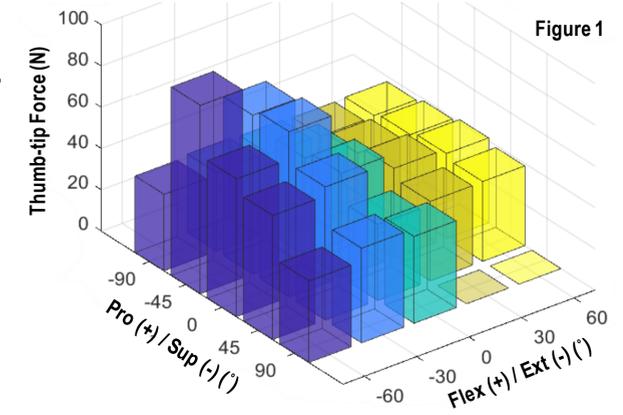


- For each posture, the maximum thumb-tip force magnitude was calculated and compared to reported experimental values [3, 4].

### Analysis

## Results & Discussion

- Maximum thumb-tip force magnitudes were plotted to examine the relationship between force and posture (Fig. 1).
- Simulations demonstrated **lower pinch force magnitude during wrist flexion** in forearm postures in the range of -45° to 45°.
  - This result is exemplified by the **80% difference in pinch force between peak wrist extension and flexion at forearm 45° pronation**.
  - Validity of this result is supported by literature, which demonstrates up to a **40% decrease in pinch force between a neutral and flexed wrist posture** [3,4].
- Simulations demonstrated **neutral and supinated wrist postures resulted in up to 20% larger pinch strengths on average compared to pronated postures**.
  - This result is supported by experimental literature reporting the greatest pinch force in a neutral forearm posture [4].



- Comparing trends across postures between simulated and experimental results was another important part of the analysis (Fig. 2).
- Simulations demonstrated a **decrease in pinch force from neutral wrist posture to complete wrist flexion** at a neutral forearm posture.
  - The validity of this result is supported by literature, which demonstrates a **similar decrease in force generation** and asserts that flexion results in decreased pinch force [3,4].
- Simulations demonstrated that an **extended wrist resulted in lowered pinch force** compared to force generated in the neutral wrist posture at a forearm posture of 90°.
  - This result is supported by experimental data reporting that the **greatest pinch force occurs at a neutral wrist posture** [4].
  - Data showing force generated during lateral pinch with a flexed wrist at a forearm posture of 90° was not collected due to inability to run simulations at these postures.

## Conclusions

- Through our simulations, we demonstrate our model's ability to generate physiologically reasonable force data. This is an important step toward creating a model capable of predicting which postures result in suboptimal force generation.
- Our model indicates that changing wrist posture results in lower force generation. This greater force generating requirement relative to a neutral wrist posture is consistent with the literature [3,4].
- Future work will involve varying muscle activations across postures to further improve the model's predictive power.

## References

[1] Nichols, et al. (2017) *J Biomech.* 58:97-104.  
 [2] Saul, et al. (2015) *Comput Methods Biomech Biomed Eng.* 18:1445-58.  
 [3] Imrhan S.N. (1991) *Appl Ergon.* 22(6):379-384.  
 [4] Halpern, et al. (1996) *J Hum Ergol.* 25(2):115-130.